

# Particle Flow Control by Magnetically Induced Dynamics of Particle Interactions

F. Wittbracht, A. Weddemann, A. Auge, A. Hütten

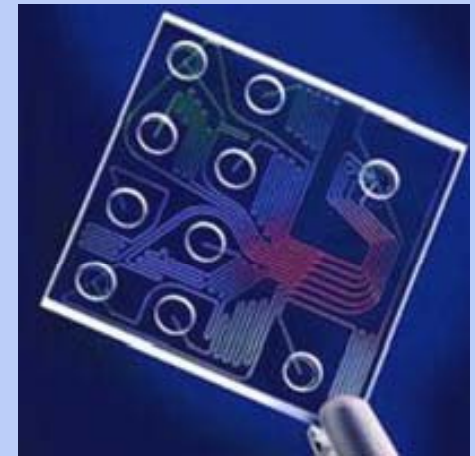
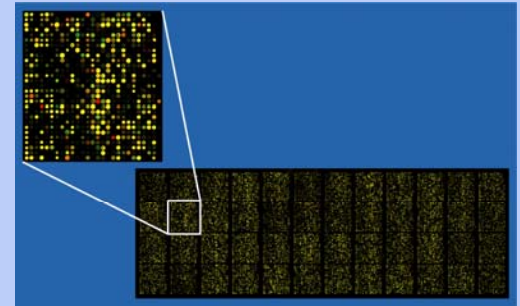
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# Motivation

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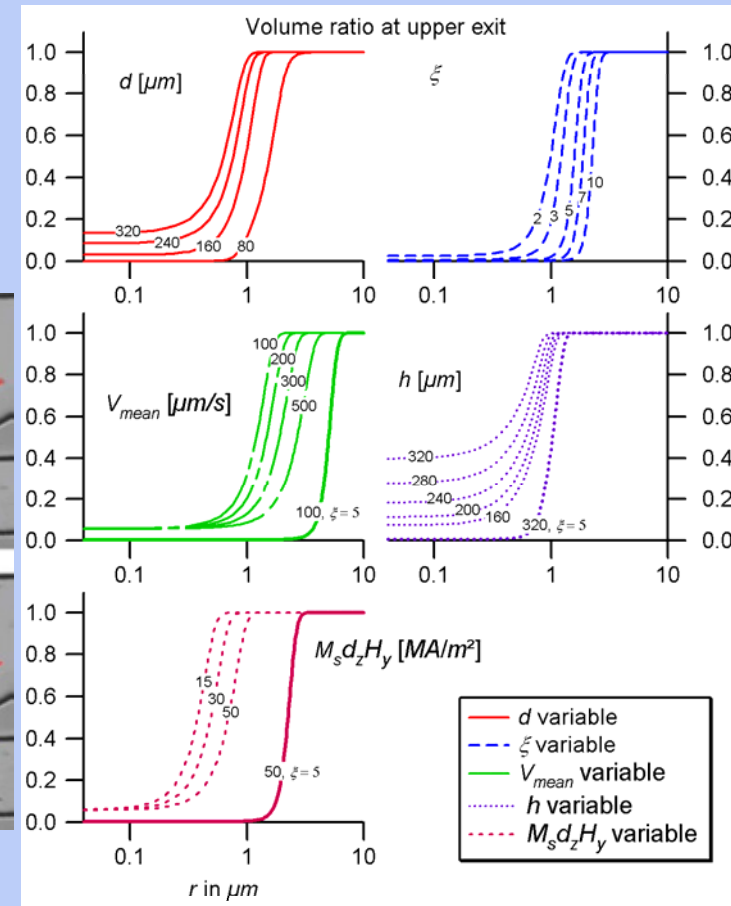
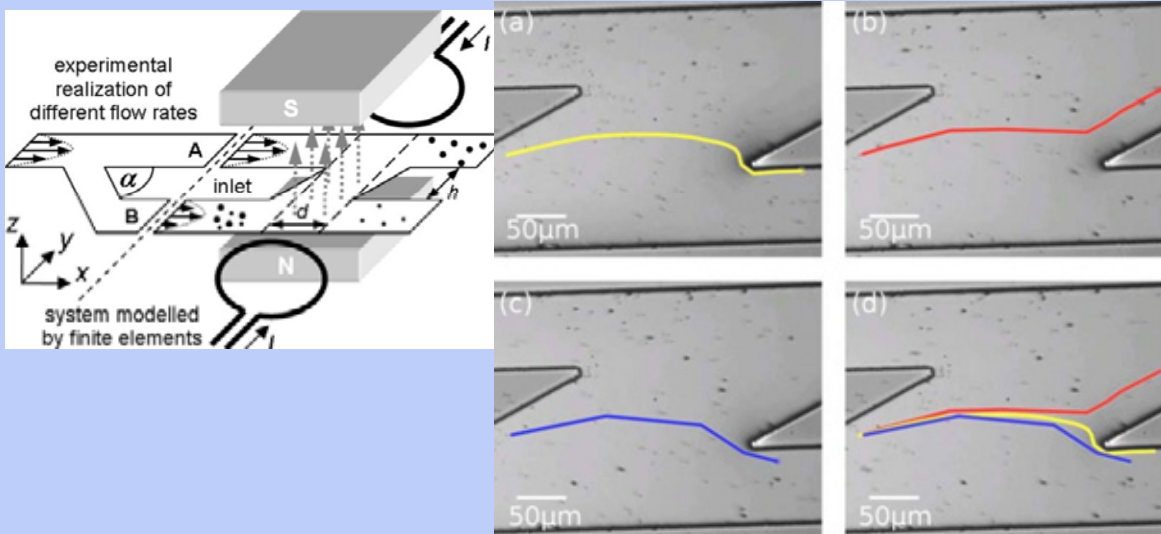
- Lab on a Chip (LOAC)
- Scaling down of single or multiple lab processes to a chip-format
- Application examples:
  - ▣ DNA sequencing
  - ▣ Electrophoresis
  - ▣ Blood sample preparation
- Two different types:
  - ▣ Microarrays
  - ▣ Microfluidics



# LOAC + Magnetism

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- Separation of magnetic beads in microfluidic systems

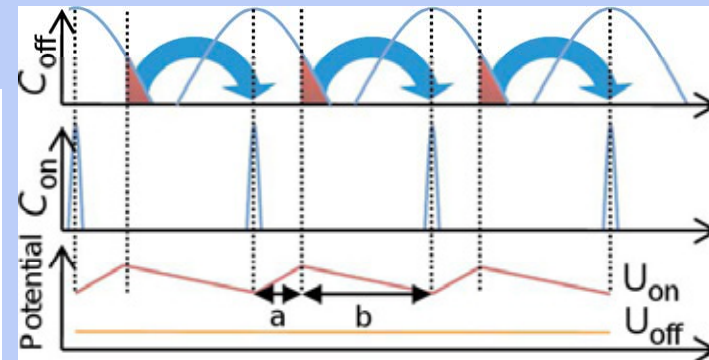
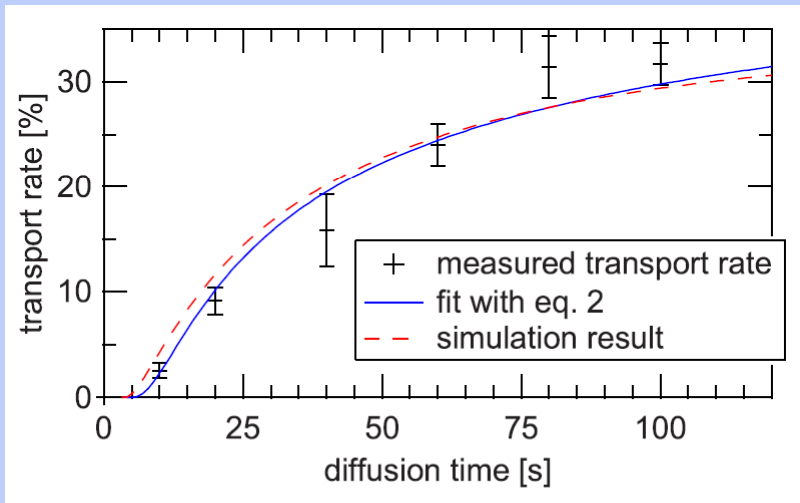


A. Weddemann et al., Appl. Phys. Lett. **94**, 173501 (2009)

# LOAC + Magnetism

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## ■ Magnetic ratchet



A. Auge et al., Appl. Phys. Lett. **94**, 183507 (2009)

So far:

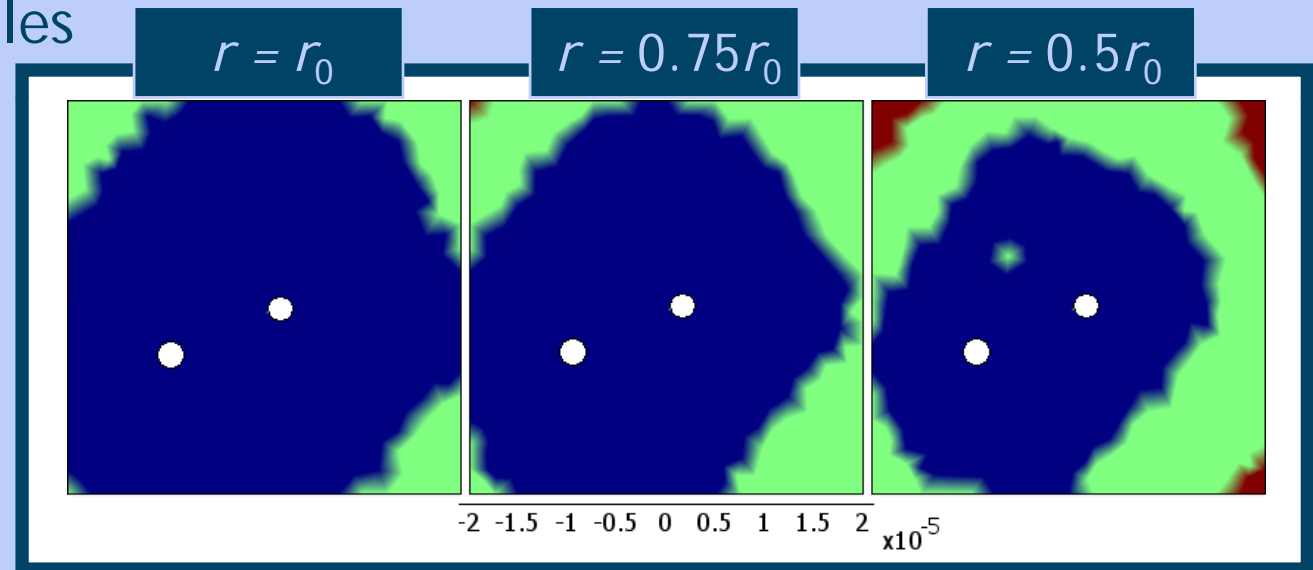
- Interaction of particles omitted
- Low-concentration limit

# Particle interactions

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Basic ideas

- Important for high throughput methods
- Interacting particles can behave in a different way than single particles



A. Weddemann, A. Auge, F. Wittbracht, S. Herth, A. Hütten, Proc. Europ. COMSOL Conf. Hannover 2008, ISBN 978-0-9766792-8-8

→ New strategies for manipulation and guidance of magnetic particles

# Governing equations

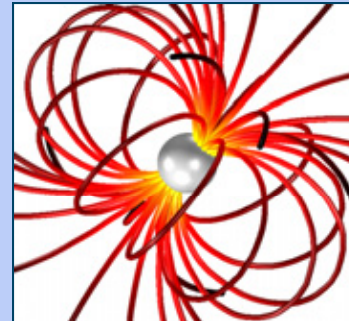
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- Particle motion

$$m \frac{dv}{dt} = F_{mag} + F_{hyd}$$

- Magnetic field  $H$  created by a magnetic moment  $m$

$$H_{part}^1(r) = \frac{1}{4\pi} \left( \frac{3 \langle m_{part}^1, r \rangle r}{|r|^5} - \frac{m_{part}^1}{|r|^3} \right)$$



- Force on a second magnetic  $m$  moment close by

$$F_{mag}^{21} = \mu_0 (m_{part}^2 \cdot \nabla) H_{part}^1$$

- Susceptibility of the surrounding medium omitted



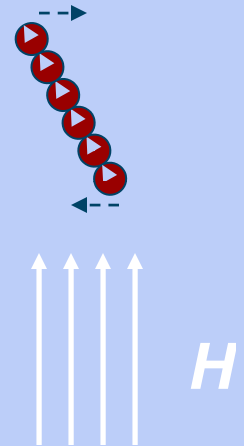
# Governing equations

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- Magnetic moment  $m$  in a field  $H$  feels a torque

$$\tau = \mu_0 m \times H$$

- strong external fields:  $m \parallel H_{\text{ex}}$
- remagnetization processes on nanosecond time scale: perfect alignment with  $H_{\text{ex}}$  even for time dependent external fields



- Stokes equation  $\eta \Delta u = -\nabla p$

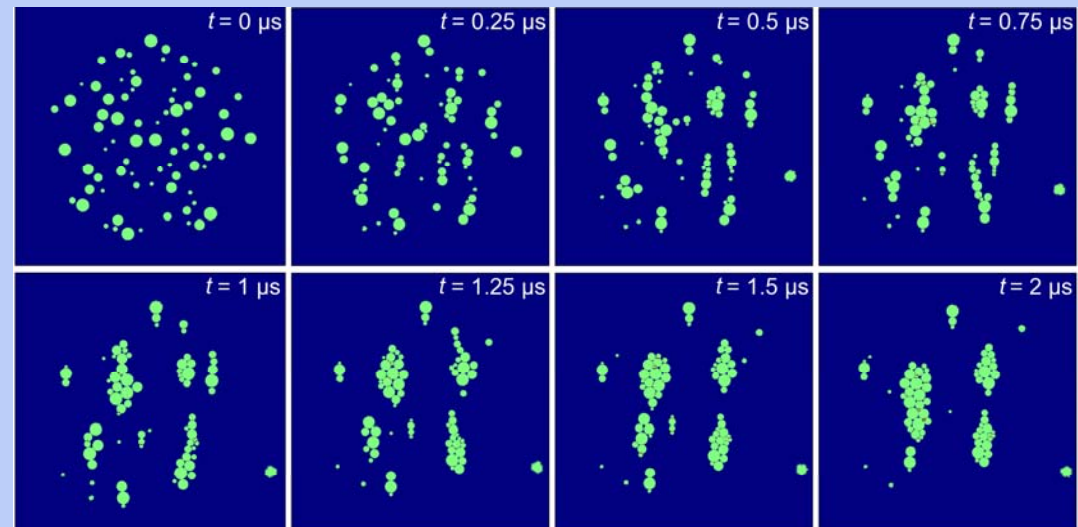
# Simulation results

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Particle agglomerates

## ■ Spatial particle distribution

- particle sizes:  $0.5\text{-}1\ \mu\text{m}$
- saturation magnetization:  $1000\ \text{kA/m}$



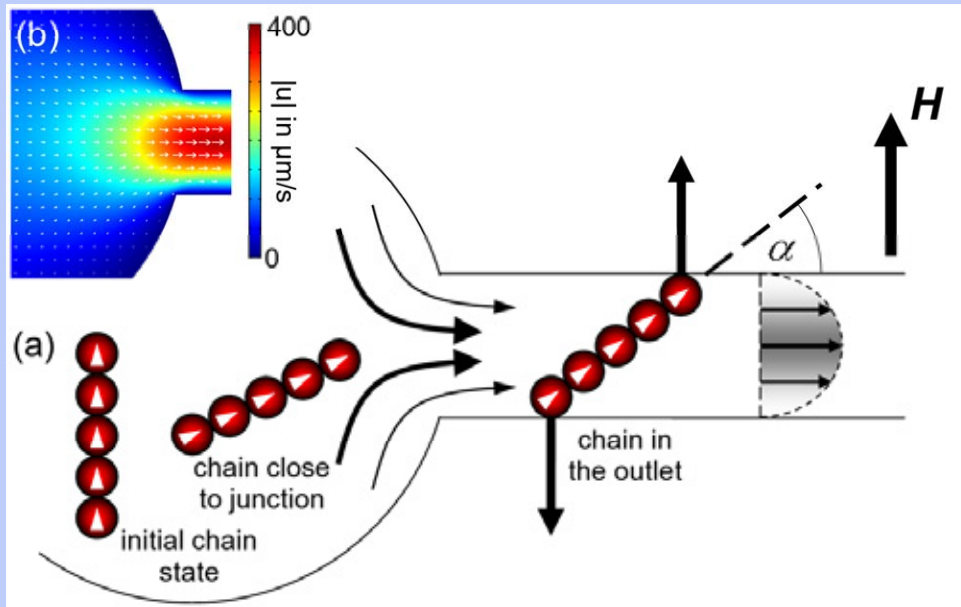
- usually no chain breaking due to flow induced shear stress
- Changing the field direction  $\rightarrow$  chain rotation low frequencies  
 $\rightarrow$  Clusters travel as confined objects



# Simulation results

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reservoir-channel junction

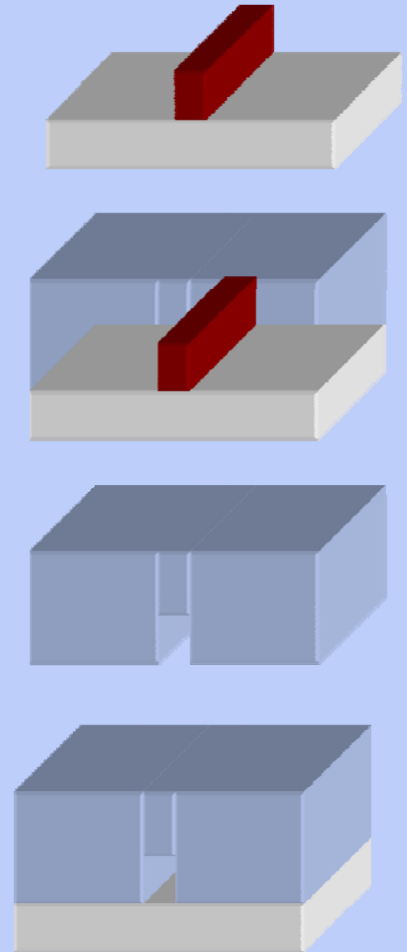


- for inhomogeneous velocity fields, the chain orientation can differ from the field direction

# Experimental realization

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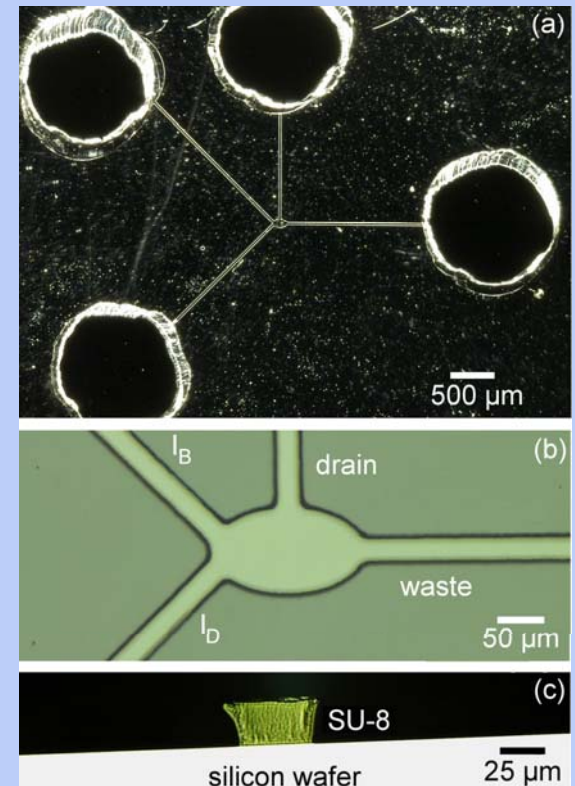
- Sample preparation:
  - Optical lithography
  - Soft lithography
  
- Oxygen plasma treatment to ensure proper sealing



# Experimental realization

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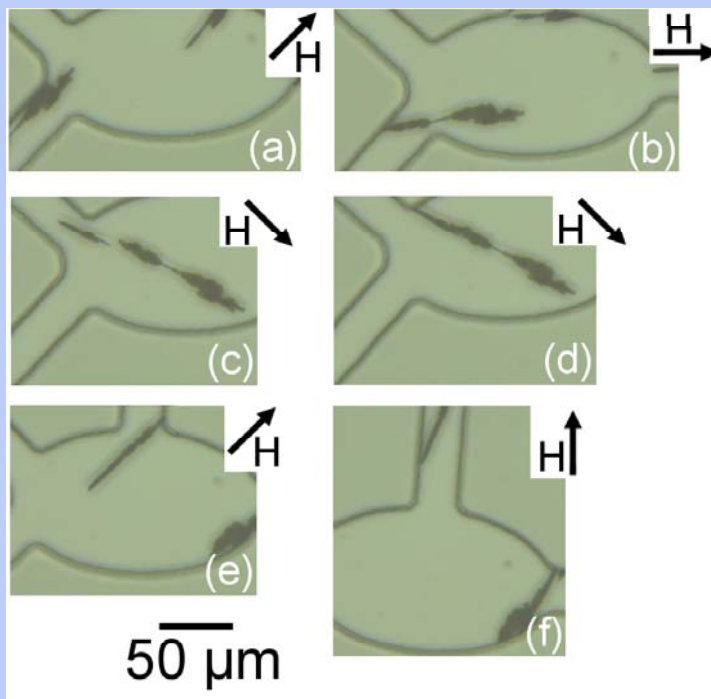
- coils for generation of in-plane homogeneous magnetic field (macroscale)
- pivotable sample holder
- digital optical microscope
- Dynabeads MyOne ( $d = 1.05 \mu\text{m}$ ) and M-280 ( $d = 2.8 \mu\text{m}$ )



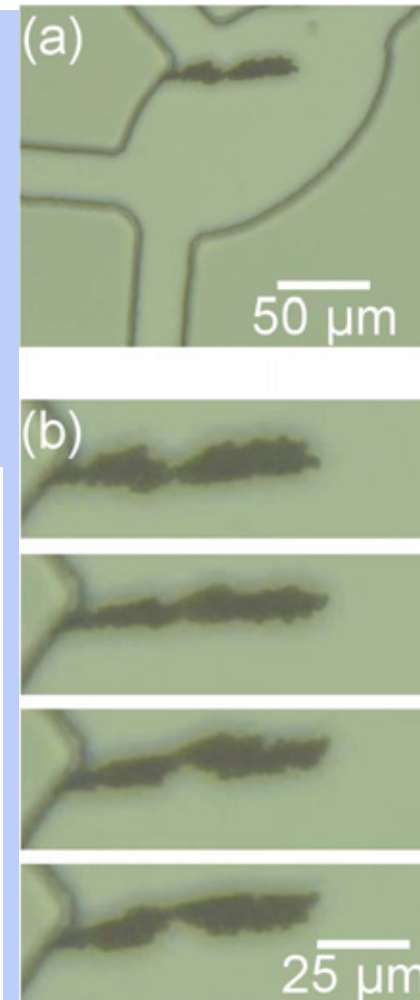
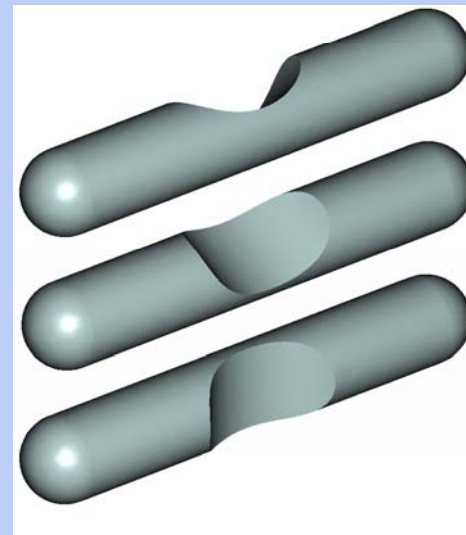
# Experimental results

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- direction of the magnetic field controls particle flow



- Self-ordering due to magnetic and hydrodynamic forces



# Conclusion & Outlook

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PHYSICS

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[www.spinelectronics.de](http://www.spinelectronics.de)

## Conclusion

- Deduce guidelines from FEM simulations
- Experimental realization of flow guidance using particle-particle interactions
- No electromagnetic components on the microscale needed

## Outlook

- New microfluidic devices using particle interactions
  - GMR/TMR sensor intergration
    - “Detection of magnetic particles by magnetoresistive sensors” by A. Weddemann
- Electromagnetics and Optics I,  
4:45 pm